# **IN.PACT DCB**

# Science Behind the Outcomes

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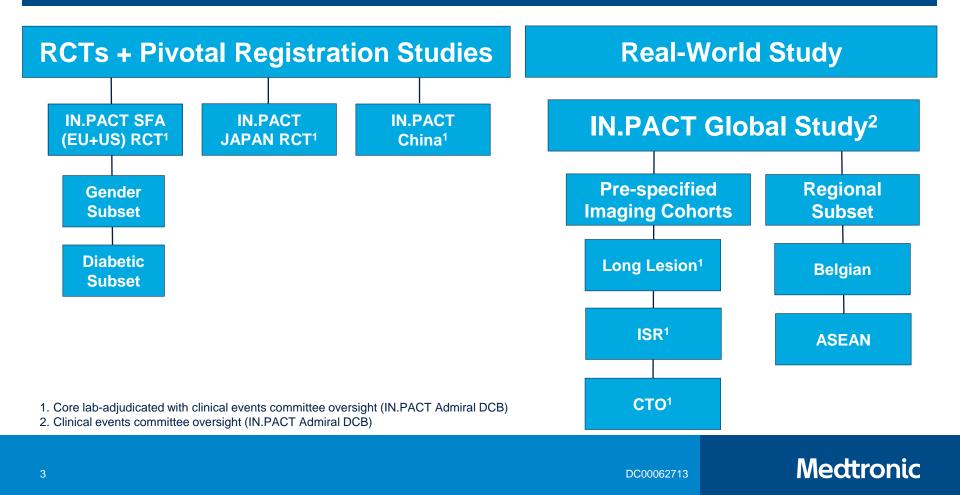
### **SFA Treatment**

- SFA disease remains a challenge to manage with no uniformly accepted evidence-based standard
- PTA is associated with high incidence of restenosis when used for anything but focal, noncomplex lesions
- Reported long-term patency rates with stents range from 60-75%,<sup>1,2</sup> but concerns persist about in-stent restenosis and stent fractures
- While drug-coated balloons (DCBs) have demonstrated promising results at 1- and 2-years in randomized trials,<sup>3-5</sup> long-term data for commercially available DCBs are limited.
- 1. Dake MD, et al. J Am Coll Cardiol 2013;61:2417-27.
- 2. Rocha-Singh KJ, et al. Catheter Cardiovasc Interv 2015;86: 164-70.
- 3. Presented by Laurich C, SVS Chicago, USA 2015.
- 4. Laird J, et al., J Am Coll Cardiol 2015;66:2329-38.
- 5. Presented by Brodmann M, VIVA Las Vegas, USA 2017.

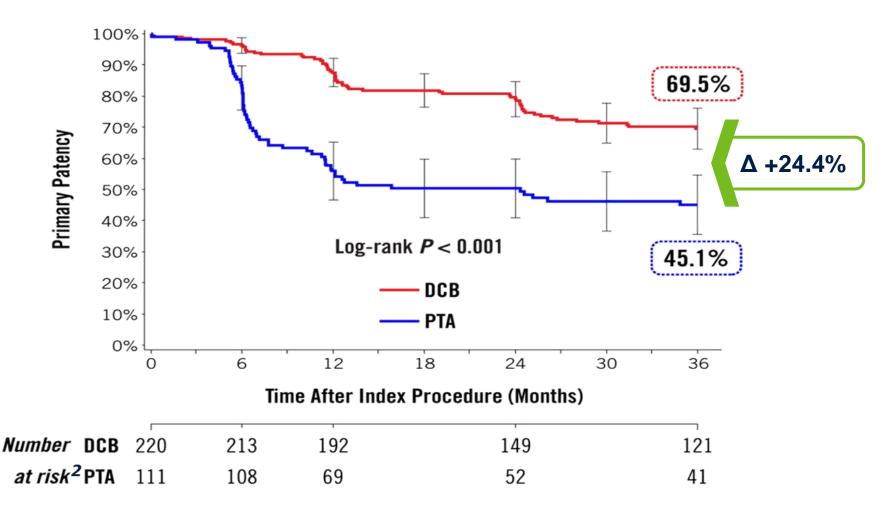
# **IN.PACT DCB SFA Clinical Program**

**Robust Adjudicated Series of 1837 Subjects** 





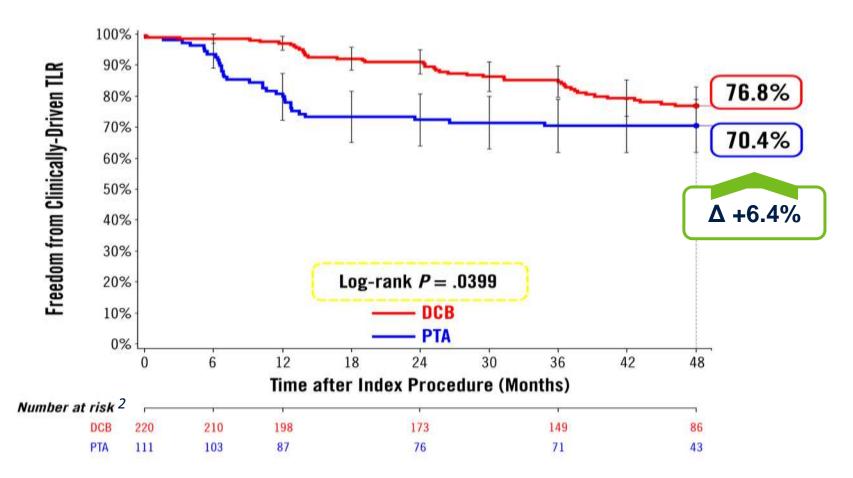
### IN.PACT SFA Trial: Primary Patency<sup>1</sup> through 3 Years



1. Freedom from core laboratory-assessed restenosis (duplex ultrasound PSVR ≤2.4) or clinically-driven target lesion revascularization through 36 months (adjudicated by a Clinical Events Committee blinded to the assigned treatment).

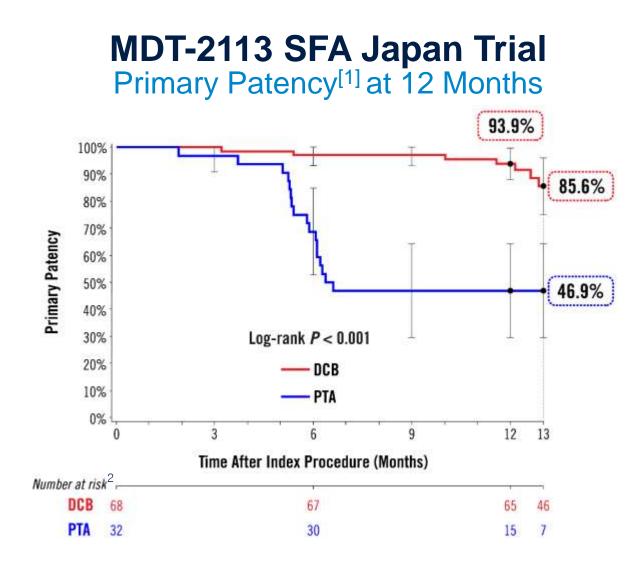
2. Number at risk represents the number of evaluable subjects at the beginning of each 30-day window.

### IN.PACT SFA Trial: Freedom from CD-TLR<sup>1</sup> through 4 Years



1. Clinically-driven TLR adjudicated by an independent Clinical Events Committee, blinded to the assigned treatment based on any re-intervention at the target lesion due to symptoms or drop of ABI of ≥20% or >0.15 when compared to post-procedure baseline ABI.

2. Number at risk represents the number of evaluable subjects at the beginning of each 30-day window.

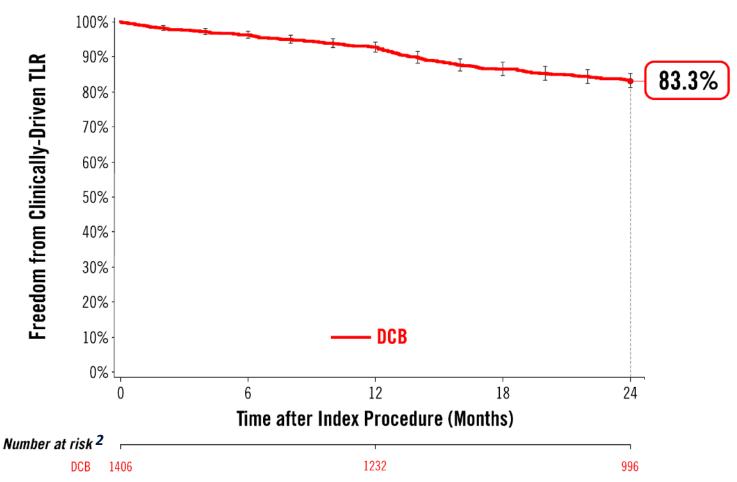


1. Freedom from core laboratory-assessed restenosis (duplex ultrasound PSVR ≤2.4) and clinically-driven target lesion revascularization through 12 months (adjudicated by a Clinical Events Committee blinded to the assigned treatment)

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2. Number at risk represents the number of evaluable subjects at the beginning of the 30-day window prior to each follow-up interval

### IN.PACT Global Study: 24-month Freedom from CD-TLR<sup>1</sup>



1. Clinically-driven TLR adjudicated by an independent Clinical Event Committee, based on any re-intervention at the target lesion due to symptoms or drop of ABI of ≥20% or >0.15 when compared to post-procedure baseline ABI.

2. Number at risk represents the number of evaluable subjects at the beginning of each 60-day window.

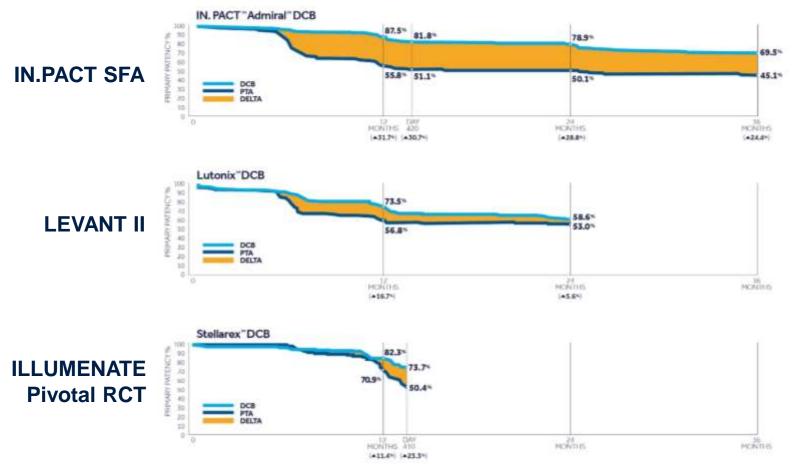
### 12-month Results across IN.PACT Admiral DCB Clinical Studies

	RCTs		Pivotal	GLOBAL						
			Registration Study		Pre-Specified Imaging Cohorts				Regional Subset	
	IN.PACT SFA <sup>1</sup>	IN.PACT Japan <sup>2</sup>	IN.PACT China <sup>3</sup>	IN.PACT Global⁴	IN.PACT Global Long Lesion Imaging Cohort <sup>5</sup>	IN.PACT Global ISR Imaging Cohort <sup>6</sup>	IN.PACT Global CTO Imaging Cohort <sup>7</sup>	IN.PACT Global Belgium Subset <sup>8</sup>	IN.PACT Global ASEAN Subset <sup>9</sup>	
Ν	220	68	143	1406	157	131	126	305	114	
Lesion Length (Mean ± SD, cm)	8.9 ±4.5	9.2 ± 5.9	10.4 ± 6.5	12.1 ± 9.5	26.4 ± 8.6	17.2 ± 10.5	22.8 ± 9.8	9.5 ± 7.9	17.4 ± 12.3	
Primary Patency (KM @ 360 days)	87.5%	93.9%	90.9%	NA	91.1%	88.7%	85.3%	NA	NA	
Primary Safety Endpoint	95.7%	95.6%	99.3%*	92.1%	94.0%	91.1%	87.7%	90.6%	96.2%	
CD-TLR	2.4%	2.9%	2.9%	7.5%	6.0%	7.3%	11.3%	7.6%	2.9%	
Major Target Limb Amputation	0.0%	0.0%	0.0%	0.2%	0.0%	0.0%	0.0%	0.7%	0.0%	
Thrombosis	1.4%	0.0%	2.2%	2.9%	3.7%	0.8%	4.3%	3.8%	0.9%	
<ol> <li>lida et al., JEVT 2018</li> <li>Chen, Z, VEITH 2017</li> <li>Jaff, M. VIVA 2016</li> </ol>	2.       lida et al., JEVT 2018       7.       Tepe, G. Charing Cross 2016         3.       Chen, Z, VEITH 2017       8.       DeLoose, K LINC 2017									

5. Scheinert, D. EuroPCR 2015.

\*30-day Safety composite

### DCB Pivotal Trial Comparisons: Primary Patency of FDA-Approved DCBs<sup>1</sup>



- 1. Primary patency and target lesion revascularization (TLR) rates may be calculated differently, and therefore may not be directly comparable; chart is for illustration only.
- IN.PACT SFA Trial values represent IN.PACT™ Admiral™ DCB arm as evaluated by 36-mo Kaplan-Meier, patency defined as PSVR ≤ 2.4 and freedom from TLR defined here as clinicallydriven TLR; IN.PACT Admiral Instructions for Use M052624T001 Rev 1F.
- 3. LEVANT II values represent Lutonix 035 arm as evaluated by 730-day Kaplan-Meier, patency defined as PSVR ≤ 2.5 and freedom from TLR defined here as all TLR; Lutonix 035 Instructions for Use BAW1387400r3..
- ILLUMENATE RCT Pivotal values represent Stellarex as evaluated by 410-day Kaplan-Meier, patency defined as PSVR ≤ 2.5 and freedom from clinically-driven TLR; Stellarex Instructions for Use No. P011966-C Rev 07/2017.



# Drug-Coated Balloons Seeing the Differences through the Mechanisms of Action



# **Drug-Coated Balloon (DCB) System**

#### **IN.PACT™ Admiral™ DCB**

Platform	Admiral <sup>™</sup> PTA balloon 4-7 mm diameters 40, 60, 80, 120, 150 mm lengths <sup>1</sup>			
Drug	<b>Paclitaxel</b> Proven anti-proliferative drug 3.5 µg/mm <sup>2</sup>			
Excipient	<b>Urea</b> Facilitates drug transfer Naturally occurring, non-toxic			
Process	<b>Medtronic</b> Reliable, scalable, uniform drug coating process			

1. The IN.PACT<sup>™</sup> Admiral<sup>™</sup> 120 and 150 mm long balloons have 4,5 & 6 mm diameters only.

### Medtronic

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### Key Elements of IN.PACT<sup>™</sup> Admiral<sup>™</sup> Design Providing over 180 days of Therapeutic Drug Levels<sup>1</sup>

### Balloon

- Coated with matrix in semi-inflated state, then wrapped
- Protects majority of matrix within folds
- Moderates urea dispersion and paclitaxel transfer

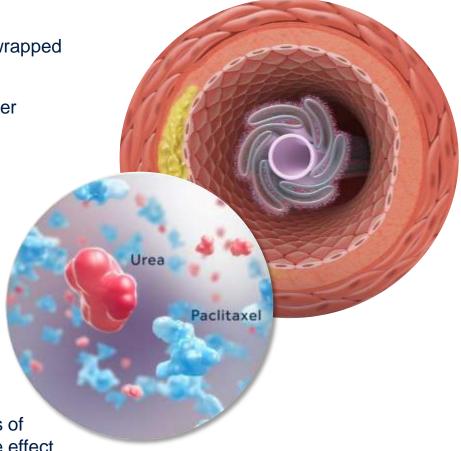
#### Urea

- Naturally occurring molecule
- Hydrates during contact with blood
- Facilitates drug transfer

#### Paclitaxel

- Proven anti-proliferative drug
- 3.5 μg/mm<sup>2</sup>
- Embedded solid phase drug provides reservoirs of soluble phase drug which exert anti-proliferative effect

1. Data on file at Medtronic (GLP Study FS208; GLP Study PS516).



# **Design Summary of the FDA-Approved DCBs**

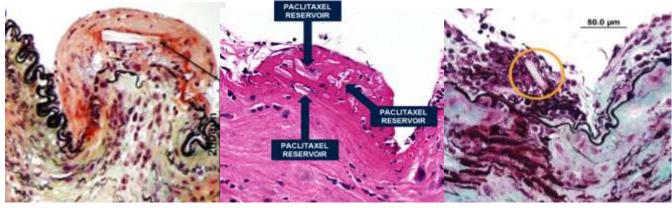
Excipient is critical in delivering and sustaining paclitaxel in the tissue.

- All three devices use paclitaxel dosing significantly lower than other medical applications<sup>1</sup>
- Excipient is unique to each DCB

	Drug (Dose)	Excipient			
IN.PACT™ Admiral™ DCB	Paclitaxel (3.5µg/mm <sup>2</sup> )	Urea			
Lutonix <sup>™*</sup> 035 DCB	Paclitaxel (2.0µg/mm <sup>2</sup> )	Polysorbate-Sorbitol			
Stellarex <sup>™*</sup> DCB	Paclitaxel (2.0µg/mm <sup>2</sup> )	Polyethylene Glycol			

1. Ng, Vivian. Eur J Clinical Investigation 2015;45(3):333-345

# Proposed Mechanism of **Action**



PACCOCATH (2009) Granada JF. Open Heart. 2014 **IN.PACT** 

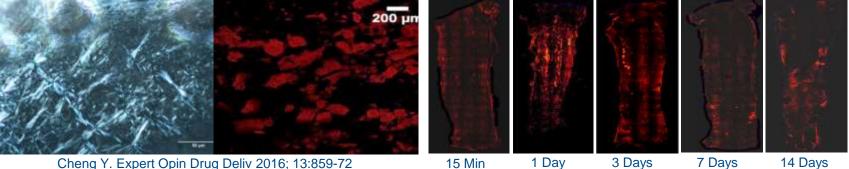
**STELLAREX** 

### Particle Type, Adhesion and Solubility Determines Tissue **Pharmacokinetics**

#### **STELLAREX (SPECTRANETICS)**



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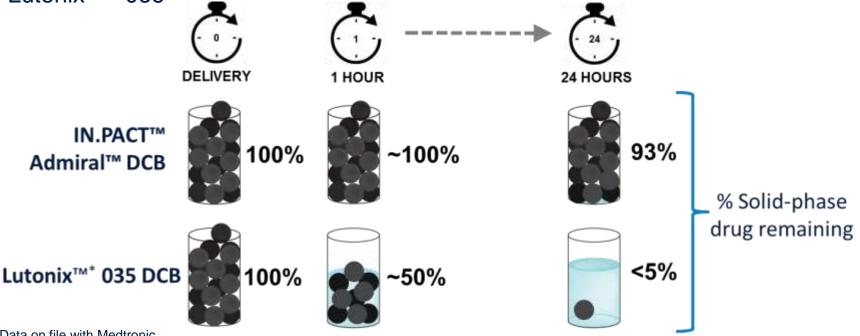


Cheng Y. Expert Opin Drug Deliv 2016; 13:859-72

# **Solid-Phase Drug Transition**

Transition from solid- to soluble-phase is different through 24 hours.<sup>1-2</sup>

- Bench-top porcine plasma model reveals that both devices transfer solid-phase paclitaxel from the DCB
- Subsequent transition from solid-phase to soluble-phase occurs at different rates
- At 24 hours, IN.PACT<sup>™</sup> Admiral<sup>™</sup> DCB retains more drug in solid-phase than Lutonix<sup>™</sup>\* 035

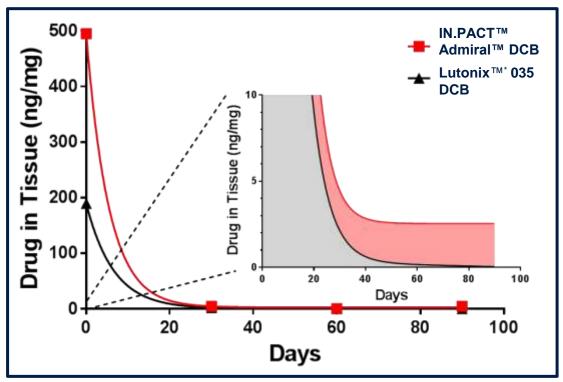


1. Data on file with Medtronic.

2. Virmani R, "Arterial wall response to drug-coated balloon use" presented at Charing Cross, London 2016.

## **Sustained Drug Availability**

Higher percentage of solid-phase drug is associated with higher drug tissue concentration through 90 days.<sup>1-2</sup>



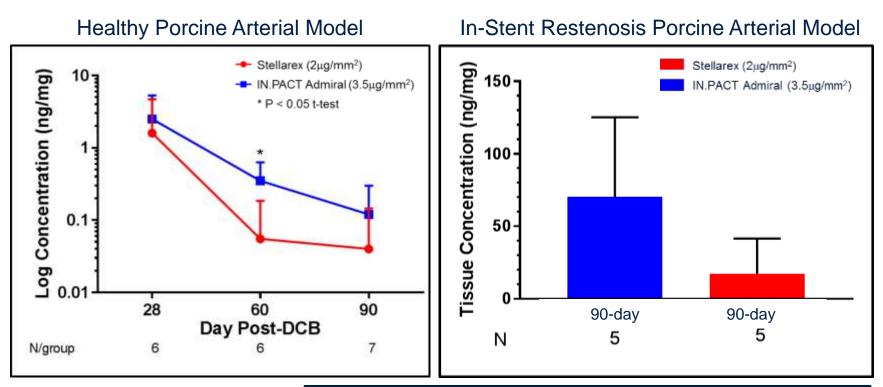
In vivo porcine model used to quantify sustained drug residence in tissue

1.Data on file with Medtronic; Study PS747.

2. Virmani R, "Arterial wall response to drug-coated balloon use" presented at Charing Cross, London 2016.

# **Sustained Drug Availability**

Different tissue drug concentrations are also demonstrated in a similar head-to-head experiment as well as porcine arterial neointima model.<sup>1,2</sup>

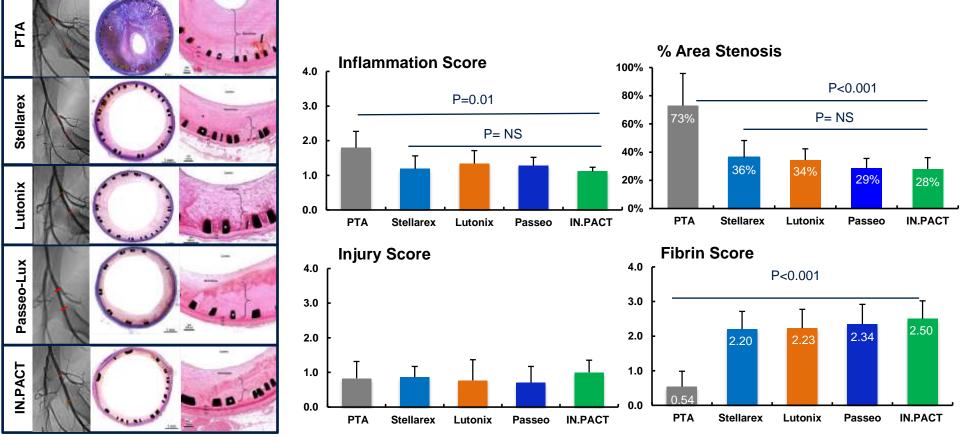


Higher input drug concentration facilitates greater long-term concentrations.

1.Data on file with Medtronic; Study PS767. 2.Data on file with Medtronic; Study PS781.

### <u>SHORT-TERM</u> Restenosis Prevention Following DCB Treatment in the FHS Model of SFA-ISR

28-Days Following ISR Treatment

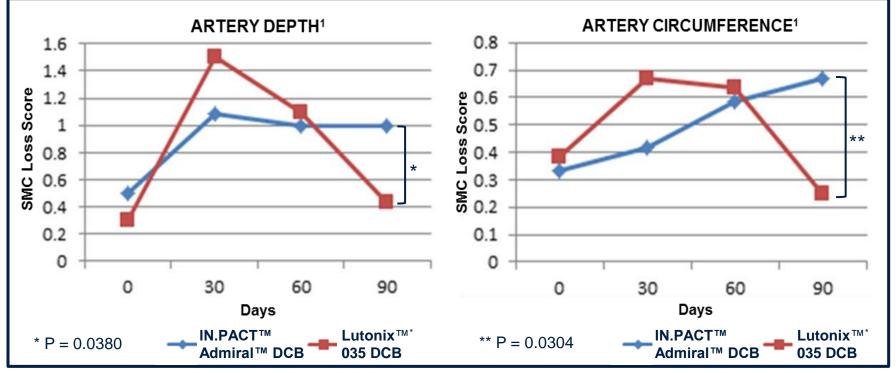


Data Courtesy of Cheng YP. Skirball Center for Innovation 2017

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# **Prolonged Anti-Proliferative Effect**

Higher percentage of solid-phase drug is associated with continued trend of smooth muscle cell loss through 90 days.<sup>1-2</sup>

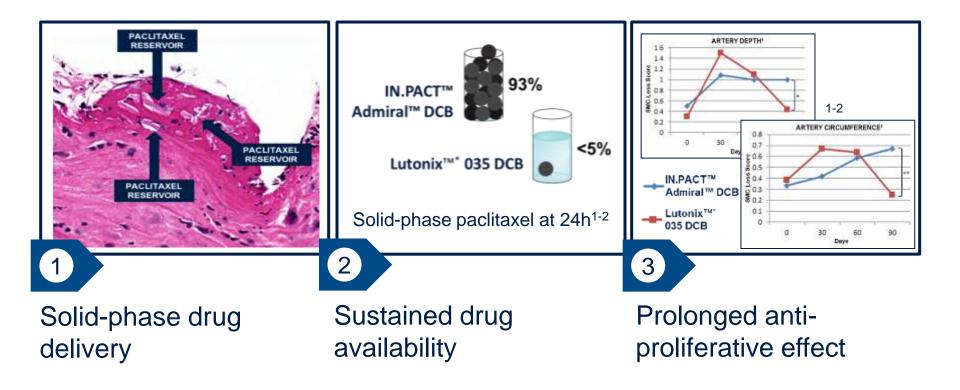


In vivo porcine model used to quantify smooth muscle cell loss through 90 days

1. Data on file with Medtronic; PS747.

2. Virmani R, "Arterial wall response to drug-coated balloon use" presented at Charing Cross, London 2016.

# **Keys to Sustained Effect**



1. Data on file with Medtronic. Ninety-day differences in artery depth delta and artery circumference demonstrate p=0.0380 and p=0.0304, respectively (right panel).

2. Virmani R, "Arterial wall response to drug-coated balloon use" presented at Charing Cross, London 2016.

Medtronic

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### Key Safety Metrics: 12-Month FDA-Approved DCB Cohorts

	LEVANT II <sup>1</sup>		Global <sup>2</sup>	IN.PACT	SFA <sup>3</sup>	Global Clinical Cohort <sup>4</sup>	EU	RCT <sup>5</sup>	US P	ivotal <sup>6</sup>	Global <sup>7</sup>
	ΡΤΑ	Lutoi	nix 035	ΡΤΑ	IN.PACT Admiral		ΡΤΑ	Stellarex	ΡΤΑ	Stellarex	Stellarex
Subjects	160	316	691	111	220	1406	72	222	100	200	371
All Thrombosis				3.7% (4/107)	1.4% (3/207)	2.9% (38/1311)			0.0% (0/95)	1.1% (2/189)	
Revasc. due to Thrombosis	0.7% (1/140)	0.4% (1/285)	1.3% (8/634)								
Major Amputation	0.0% (0/140)	0.3% (1/286)	0.5% (3/635)	0.0% (0/107)	0.0% (0/207)	0.2% (3/1311)	0.0% (0/60)	0.0% (0/204)	0.0% (0/95)	0.0% (0/189)	17

Consistently low frequency of thrombosis and major amputation across platforms.

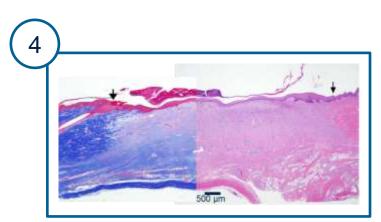
Does distal downstream particle embolization impact wound healing and could affect clinical outcomes?

### Paclitaxel Effect on Wound Healing Experimental Design

- 1. Wound creation
- 2. Bilateral treatment PTA or DCB x1 or DCB x3
- 3. Clinical assessment

Scoring and wound care (dressing change) three times per week

4. Termination (14 and 28 days)
 Histopathological assessment
 Quantification of drug in tissue





### Wound Healing Clinical Evaluation



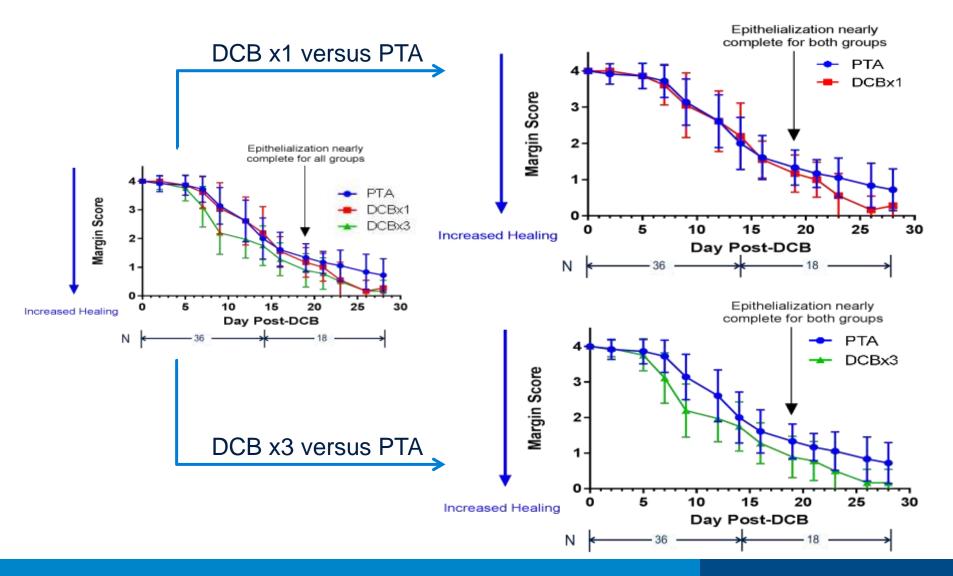
#### Wound healing (Three times per week)

- Modified Draize wound healing score rank (0-4)
- Modified Hollander Cosmesis score rank (0-4)

#### Histopathology (14 & 28 days)

- Re-epithelialization
- Collagen deposition or scar formation
- Neovascularization or granulation
- Wound contraction and/or inflammation

### Wound Healing Hollander Score: Direct Indicator of Wound Closure



### Conclusions

- There does not appear to be a Class Effect in DCBs
- The In.Pact Admiral is the only DCB to demonstrate a superior treatment effect over PTA through four years
- Continued safety of IN.PACT<sup>™</sup> Admiral<sup>™</sup> DCB through <u>four years</u>
- The ability to maintain a sustained biological response over time appears to be the main driver of clinical success of DCBs
- Not only paclitaxel dosing but also particle solubility are important technological drivers to achieve long-term suppression of restenosis
- Particulate embolization does not seem to affect wound healing at the experimental level, its effect in humans requires further studies

# **Thank You!**

